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(54) WEDGE COUPLING

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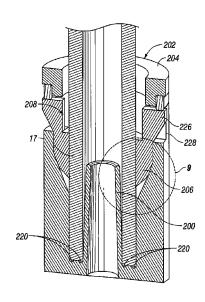
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(57) ABSTRACT

A wedge coupling for coupling a tubing to a housing is disclosed. The wedge coupling includes a base having an opening defined therein and configured to receive a portion of the tubing therethrough and a plurality of prongs disposed on the base and around an inner periphery of the opening. The plurality of prongs are configured to slidably engage the housing and to deflect inwardly to secure the tubing to a nozzle adapter disposed within the housing.

8 Claims, 6 Drawing Sheets



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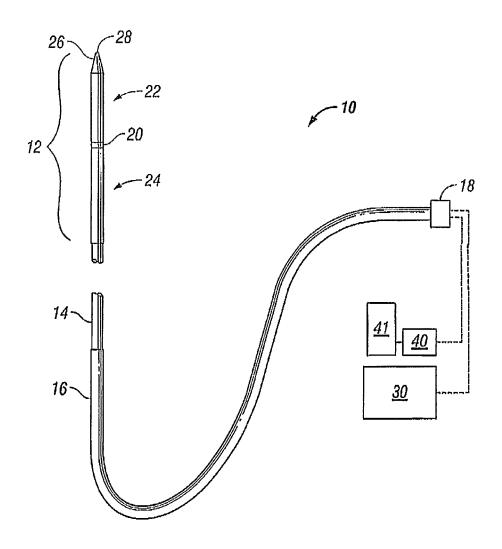


FIG. 1

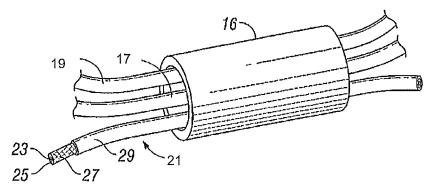


FIG. 2

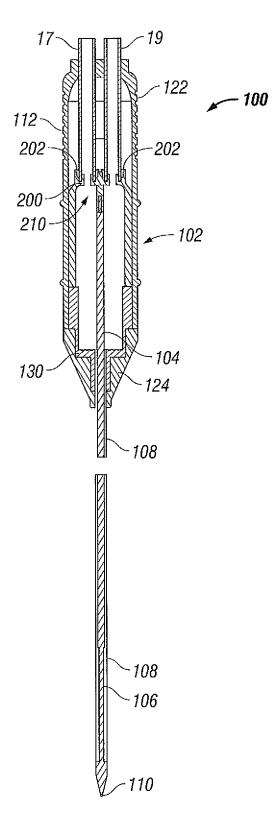


FIG. 3

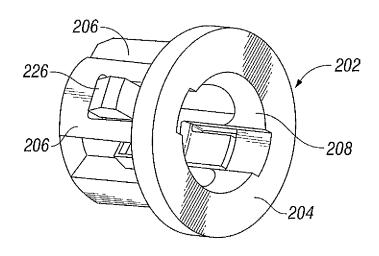


FIG. 4

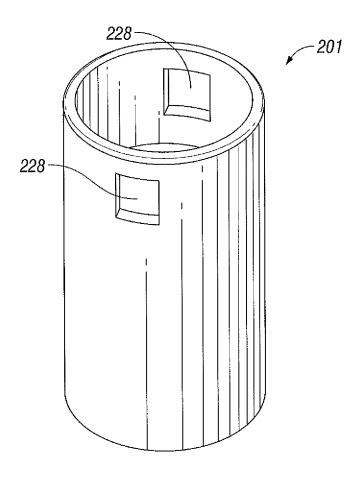


FIG. 5

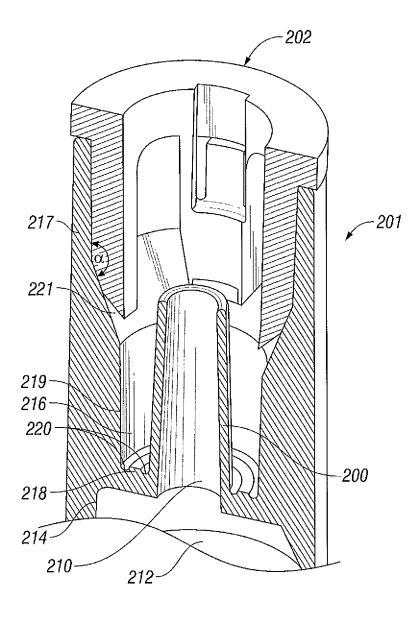


FIG. 6

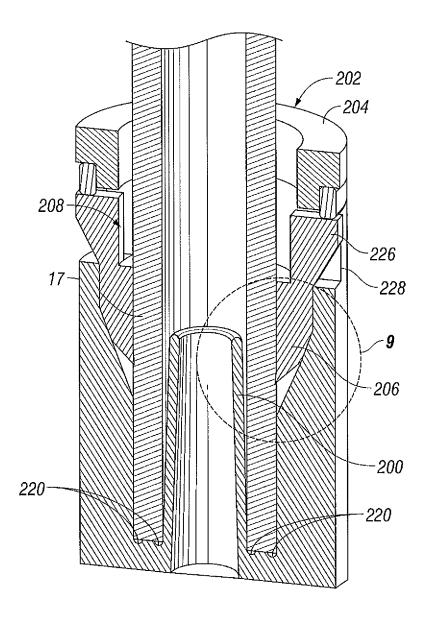


FIG. 7

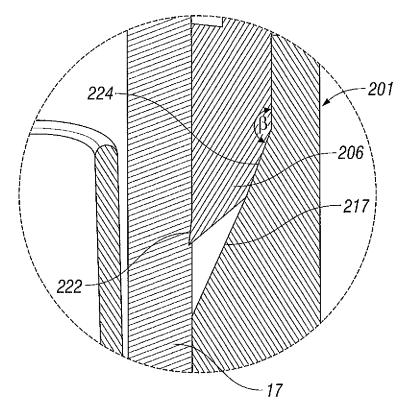


FIG. 8

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WEDGE COUPLING

CROSS-REFERENCE TO RELATED APPLICATIONS

This application claims the benefit of priority to U.S. Provisional Application Ser. No. 60/990,542 entitled "WEDGE COUPLING" filed Nov. 27, 2007 by Arnold V. DeCarlo, which is incorporated by reference herein.

BACKGROUND

1. Technical Field

The present disclosure relates generally to ablation syssystem and method for coupling a flexible conduit to ablation probes, liquid supplies, gas supplies, etc.

2. Background of Related Art

Treatment of certain diseases requires destruction of malignant tissue growths (e.g., tumors). It is known that 20 tumor cells denature at elevated temperatures that are slightly lower than temperatures injurious to surrounding healthy cells. Therefore, known treatment methods, such as hyperthermia therapy, heat tumor cells to temperatures above 41° C., while maintaining adjacent healthy cells at lower tempera- 25 tures to avoid irreversible cell damage. Such methods involve applying electromagnetic radiation to heat tissue and include ablation and coagulation of tissue. In particular, microwave or radiofrequency energy is used to coagulate and/or ablate tissue to denature or kill the cancerous cells. Energy is applied 30 via ablation antenna probes which penetrate tissue to reach tumors. There are several types of ablation probes.

In certain procedures it is desirable to provide liquid to the ablation probe. The liquid may be used as a coolant to reduce the temperature at the tip of the probe in order to maintain the 35 desired ablation temperature. In addition, the liquid may be used a dielectric to provide for dynamic matching of a microwave ablation probe. The liquid is usually provided to the probe via tubing.

SUMMARY

According to one aspect of the present disclosure a wedge coupling for coupling a tubing to a nozzle adapter within a housing is disclosed. The wedge coupling includes a base 45 having an opening defined therein and configured to receive a portion of the tubing therethrough and a plurality of prongs disposed on the base and around an inner periphery of the opening. The plurality of prongs are configured to slidably engage the housing and to deflect inwardly to secure the 50 tubing to a nozzle adapter disposed within the housing.

According to another aspect of the present disclosure an ablation probe is disclosed. The probe includes a housing having a funnel-shaped inner surface and a nozzle adapter connected thereto and a tubing configured to slide into the 55 funnel-shaped inner surface and over the nozzle adapter. The probe also includes a wedge coupling having a base with an opening defined therein and configured to receive a portion of the tubing therethrough and a plurality of prongs disposed on the base and around an inner periphery of the opening. The 60 plurality of prongs are configured to slidably engage the housing and to deflect inwardly to secure the tubing to a nozzle adapter disposed within the housing.

A method for securing a tubing to a housing is also contemplated by the present disclosure. The method includes the 65 steps of inserting a tubing into a wedge coupling that includes a base having an opening defined therein and configured to

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receive a portion of the tubing therethrough. The coupling also includes a plurality of prongs disposed on the base and around an inner periphery of the opening. The method also includes the step of inserting the tubing with the wedge coupling disposed thereon into a housing having a funnel-shaped inner surface and a nozzle adapter connected thereto, such that the tubing slides into the funnel-shaped inner surface and over the nozzle adapter and the plurality of prongs slidably engage the housing and deflect inwardly thereby securing the 10 tubing to the nozzle adapter.

BRIEF DESCRIPTION OF THE DRAWINGS

The above and other aspects, features, and advantages of tems. More particularly, the present disclosure is directed to a 15 the present disclosure will become more apparent in light of the following detailed description when taken in conjunction with the accompanying drawings in which:

> FIG. 1 is a schematic diagram of an ablation probe assembly according to the present disclosure;

FIG. 2 is a perspective view of a conduit of the ablation probe assembly of FIG. 1;

FIG. 3 are a cross-sectional view of an ablation probe cooling assembly according to one embodiment of the present disclosure;

FIG. 4 is a perspective view of a wedge coupling according to one embodiment of the present disclosure;

FIG. 5 is a perspective view of a housing according to one embodiment of the present disclosure;

FIG. 6 is a perspective cross-sectional view of the wedge coupling and the housing according to the present disclosure; and

FIGS. 7 and 8 are partial cross-sectional views of the wedge coupling and the housing according to the present disclosure.

DETAILED DESCRIPTION

Particular embodiments of the present disclosure will be described herein below with reference to the accompanying 40 drawings. In the following description, well-known functions or constructions are not described in detail to avoid obscuring the present disclosure in unnecessary detail.

The present disclosure provides for a system and method to couple various types of flexible tubing to input and/or output ports of various ablation apparatuses (e.g., a microwave probe, electrosurgical monopolar electrodes, pump, etc.). In particular, the tubing may be used in cooling systems which circulate cooling liquid through the microwave probe. FIG. 1 shows a diagram of an ablation probe assembly 10 which may be any type of probe suitable for depositing radiofrequency energy and may be used with a cooling system as described herein. The antenna assembly 10 is generally comprised of radiating portion 12 that may be coupled by feedline 14 (or shaft) via conduit 16 to connector 18, which may further connect the assembly 10 to a power generating source 30, e.g., a generator and a supply pump 40.

Assembly 10 includes a dipole ablation probe assembly. Other antenna assemblies, e.g., monopole or leaky wave antenna assemblies, may also be utilized. Distal portion 22 of radiating portion 12 may include a tapered end 26 that terminates at a tip 28 to allow for insertion into tissue with minimal resistance. In those cases where the radiating portion 12 is inserted into a pre-existing opening, tip 28 may be rounded or flat.

Proximal portion 24 is located proximally of distal portion 22, and junction member 20 is located between both portions such that a compressive force is applied by distal and proxi3

mal portions 22, 24 upon junction member 20. Placing distal and proximal portions 22, 24 in a pre-stressed condition prior to insertion into tissue enables assembly 10 to maintain a stiffness that is sufficient to allow for unaided insertion into the tissue while maintaining a minimal antenna diameter, as 5 described in detail below.

Feedline 14 may electrically connect antenna assembly 10 via conduit 16 to generator 30 and usually includes a coaxial cable made of a conductive metal, which may be semi-rigid or flexible. Feedline 14 may also have a variable length from a 10 proximal end of radiating portion 12 to a distal end of conduit 16 ranging between about 1 to 15 inches. The feedline 14 may be constructed of copper, gold, stainless steel or other conductive metals with similar conductivity values. The metals may also be plated with other materials, e.g., other conductive 15 materials, to improve their properties, e.g., to improve conductivity or decrease energy loss, etc.

As shown in FIG. 2, the conduit 16 includes a flexible coaxial cable 21 and one or more flexible tubes, inflow tubing 17 and outflow tubing 19 for supplying and withdrawing 20 cooling liquid into and out of the radiating portion 12, respectively. The cable 21 includes an inner conductor 23 (e.g., wire) surrounded by an insulating spacer 25, which is concentrically disposed within an outer conductor 27 (e.g., cylindrical conducting sheath). The cable **21** may also include an 25 outer insulating sheath 29 surrounding the outer conductor 27. The connector 18 couples the inflow and outflow tubing 17, 19 to the supply pump 40 and the cable 21 to the generator 30. The supply pump 40 is coupled to a supply tank 41 that stores the cooling liquid and maintains the liquid at a prede- 30 termined temperature. In one embodiment, the supply tank 41 may include a cooling unit that cools the returning cooling liquid from the outflow tubing 19.

The cooling fluid may be pumped using positive pressure through inflow tubing 17; alternatively, negative pressure 35 may also be used to draw the fluid out of the region through outflow tubing 19. Negative pressure through outflow tubing 19 may be utilized either alone or in conjunction with positive pressure through inflow tubing 17. Alternatively, positive pressure through inflow tubing 17 may be utilized either alone 40 or in conjunction with negative pressure through outflow tubing 19. In pumping the cooling fluid, the cooling fluid may be passed at a constant and uniform flow rate. In another variation, the flow may be intermittent such that a volume of cooling fluid may be pumped into the radiating portion 12 and 45 allowed to warm up by absorbing heat from the antenna. Once the temperature of the fluid reaches a predetermined level below temperatures where thermal damage to tissue occurs, the warmed fluid may be removed and displaced by additional cooling fluids. Temperature sensors (such as thermistors, 50 thermocouples, etc.) may be incorporated within or upon radiating portion 12 to sense the fluid and/or outer jacket temperatures. The system may be configured to automatically pump additional cooling fluid from the supply tank 41 once the sensed temperature reaches the predetermined level or it 55 may be configured to notify the user via, e.g., an audible or

The cooling fluid used may vary depending upon desired cooling rates and the desired tissue impedance matching properties. Biocompatible fluids may be included which have 60 sufficient specific heat values for absorbing heat generated by radio frequency ablation probes, e.g., liquids including, but not limited to, water, saline, liquid chlorodifluoromethane, etc. In another variation, gases (such as nitrous oxide, nitrogen, carbon dioxide, etc.) may also be utilized as the cooling 65 fluid. For instance, an aperture within the radiating portion 12 may be configured to take advantage of the cooling effects

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from the Joule-Thompson effect, in which case a gas, e.g., nitrous oxide, may be passed through the aperture to expand and cool the radiating portion 12. In yet another variation, a combination of liquids and/or gases, as mentioned above, may be utilized as the cooling medium.

FIG. 3 show a cross-sectional side view and an end view, respectively, of one variation of the antenna assembly to (e.g., antenna cooling assembly 100) that may be utilized with any number of conventional ablation probes or the ablation probes described herein, particularly the straight probe configuration as shown in FIG. 1. Although this variation illustrates the cooling of a straight probe antenna, a curved or looped ablation probe may also utilize much of the same or similar principles, as further described below.

Antenna cooling assembly 100 includes a cooling handle assembly 102 and an elongate outer jacket 108 extending from handle assembly 102. Outer jacket 108 may extend and terminate at tip 110, which may be tapered to a sharpened point to facilitate insertion into and manipulation within tissue, if necessary. Ablation probe 104 may be positioned within handle assembly 102 such that the radiating portion 106 of antenna 104 extends distally into outer jacket 108 towards tip 110. Inflow tubing 17 may extend into a proximal end of handle body 112 and distally into a portion of outer jacket 108. Inflow tubing 17 may also extend from within handle body 112 such that the distal ends of inflow tubing 17 and outflow tubing 19 are in fluid communication with one another, as described in further detail below.

As shown, handle body 112 may be comprised of proximal handle hub 122, which encloses a proximal end of antenna 104, and distal handle hub 124, which may extend distally into outer jacket 108. Proximal handle hub 122 and distal handle hub 124 may each be configured to physically interfit with one another at hub interface 130 to form a fluid tight seal. Accordingly, proximal handle hub 122 may be configured to be received and secured within a correspondingly configured distal handle hub 124 (seen in FIG. 3 as a male-female connection). Proximal and distal handle hubs 122, 124 may each be formed from the same, similar or different materials. If hubs 122, 124 are fabricated from the same material, a variety of non-conductive materials may be utilized, e.g., polymers, polyimides, plastics, etc. Alternatively, proximal handle hub 122 may be fabricated from a metal or alloy, e.g., stainless steel, platinum, nickel, nickel-titanium, etc., while distal handle hub 124 (or just the handle portion over the radiating portion of the ablation probe) may be fabricated from one of the non-conductive materials previously mentioned.

The distal ends of inflow tubing 17 and outflow tubing 19 may be positioned within handle body 112 such that fluid is pumped into handle body 112 via the pump 40 through inflow tubing 17. Fluid entering handle body 112 may come into direct contact with at least a portion of the shaft of antenna 104 to allow for convective cooling of the antenna shaft to occur. The fluid may be allowed to exit handle body 112 via inflow outflow tubing 19. In one embodiment, the outer jacket 108 may remain in direct fluid communication with inflow tubing 17 and outflow tubing 19 such that fluid contacts the antenna 104 directly along a portion of the length, or a majority of the length, or the entire length of antenna 104. Thus, the cooling assembly 100 is effective in cooling the antenna 104 directly rather than cooling the tissue surrounding the antenna 104, although the surrounding tissue may also be conductively cooled via assembly 100.

The inflow and outflow tubing 17 and 19 are inserted into their respective nozzle adapters 200. The inflow and outflow tubing 17 and 19 are secured to the adapters 200 by a wedge coupling 202 which is shown in FIG. 4. For sake of simplicity

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the wedge coupling 202 is described with respect to the inflow tubing 17. During assembly, the tubing 17 is inserted into the wedge coupling 202. Thereafter the tubing 17 along with the wedge coupling 202 disposed thereon is inserted into the housing 201 over the nozzle adapter 200. Once the tubing 17 is in place, the wedge coupling 202 is pushed into the housing 201 securing the tubing 17 within the housing 201. Additional embodiments of using the wedge coupling 202 to connect multiple tubes to multiple nozzle adapters 200 on various medical instruments and equipment is within the purview of 10 those skilled in the art.

With reference to FIGS. 4-8, the wedge coupling 202 includes a base 204, a plurality of prongs 206 extending therefrom and an opening 208 defined within the base 204 and surrounded by the prongs 206. The opening 208 has an inner 15 diameter that is substantially equal to the outer diameter of the tubing 17 allowing the wedge coupling 202 to be slidably disposed on the tubing 17 and for the tubing 17 to pass therethrough.

FIGS. 5 and 6 show tube housing 201 including the nozzle 20 adapter 200 that has an opening 210 providing access to a flow tube 212. The housing 201 also includes a funnel-shaped inner surface 216 having a proximal portion 217 and a distal portion 219 connected by a transition portion 221. The proximal portion 217 has an inner diameter larger than the diameter 25 of the distal portion 219 with the transition portion 221 having sloping walls at a predetermined angle α providing for the transition between the portions 217 and 219.

The nozzle adapter 202 is connected to an inner surface 216 of the housing 201 via a housing base 214. The outer surface 30 218 of the base 214 includes troughs 220 at the point where the adapter 202 and the inner surface 216 meet the base 214. In one embodiment, when the tubing 17 is inserted into housing 201, the pressure applied to the tubing 17 by the wedge coupling 202 forces the edges of the tubing 17 at a distal end 35 thereof to push into the base 214. This, in turn, results in the tubing 17 separating from the adapter 202. The troughs 220 provide room for the edges of the tubing 17 to spread when the tubing 17 is pushed into the housing 201 thereby relieving the pressure. This provides for a secure seal between the tubing 40 17 and the adapter 202.

With reference to FIGS. 7 and 8, the tubing 17 being inserted within the housing 201 and being secured by the wedge coupling 202 is shown. As discussed above, the wedge coupling 202 includes two or more prongs 206 disposed on 45 the base 204. The prongs 206 may be disposed in equiangular configuration such that when equal pressure is applied to each of the prongs 206 and the tubing 17, the forces cancel out and the tubing 17 is secured by the wedge coupling 202. The prongs 206 are configured to be slidably received within the 50 housing 201 and to be deflected inwards thereby to secure the tubing 17 to the nozzle adapter 200.

With reference to FIG. 8, the prongs 206 include a tooth-shaped feature 222 at a distal end thereof. In addition, the prongs 206 may include a tapered portion 224 at a predetermined angle β at the distal end thereof. The angle β of the tapered portion 224 is larger than the angle α of the transitional portion 219. Thus, the prongs 206 are forced inwardly by the housing 201 as the wedge coupling 202 is inserted therein. More specifically, as the prongs 206 are inserted into 60 the housing 201, the tapered portions 224 of the prongs 206 are in contact with the proximal portion 217. Due to the larger deflection angle of the tapered portions 224, the prongs 206 are bent inwardly against the tubing 17. The features 222 engage the outer surface of the tubing 17 and secure the 65 tubing 17 to the nozzle adapter 200. The wedge coupling 202 may be formed from any suitable material and, in some

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embodiments, materials having high tensile strength allowing the prongs 206 to bend under pressure and compress the tubing 17 thereby securing the tubing 17 within the housing 201

The wedge coupling 202 is secured to the housing 201 to prevent the wedge coupling 202 from sliding out due to the deflection of the prongs 206 by the housing 201. As shown in FIGS. 4 and 8, the wedge coupling 202 may include one or more box clips 226 that are configured to interface with corresponding windows 228 (FIG. 5). The box clips 226 may be integrally formed with and/or may be cut out within the prongs 206 allowing the prongs 206 act as a spring. The box clips 226 extend further outward than the outer surface of the prongs 206 similar to the base 204. The base 204 and the box clips 226 protrude past the proximal portion 217 of the inner surface 216. Thus, when the wedge coupling 202 is inserted into the housing 201 the base 204 rests against the proximal end of the housing 201. Similarly, the box clips 226 are compressed by the proximal portion 217 until the wedge coupling 202 is fully inserted into the housing 201. At which point, the box clips 226 are aligned with the corresponding windows 228 and the box clips 226 are deflected therein. The box clips 226 are thereafter biased against the windows 228 by the deflection of the prongs 206 and the transitional portion 219 thereby preventing the wedge coupling 202 from sliding out of the housing 201.

The described embodiments of the present disclosure are intended to be illustrative rather than restrictive, and are not intended to represent every embodiment of the present disclosure. Various modifications and variations can be made without departing from the spirit or scope of the disclosure as set forth in the following claims both literally and in equivalents recognized in law.

What is claimed is:

1. An assembly for use with an ablation probe, the assembly comprising:

- an inflow housing defining an inflow axis, and an outflow housing defining an outflow axis, the inflow housing and the outflow housing extending longitudinally along their respective axes in side-by-side relation and parallel orientation relative to one another, the inflow housing and the outflow housing each including:
 - a funnel-shaped inner surface;
 - a nozzle adapter connected to the funnel-shaped inner surface; and
 - a housing base from which the nozzle adapter extends, the housing base including at least one trough defined therein;
- an inflow tubing and an outflow tubing, each tubing configured to slide into the respective funnel-shaped inner surface and over the respective nozzle; and
- an inflow wedge coupling and an outflow wedge coupling, each including:
 - a base having an opening defined therein configured to receive a portion of the respective tubing therethrough; and
 - a plurality of prongs disposed on the respective base around an inner periphery of the respective opening, the plurality of prongs configured to slidably engage an the respective housing and to deflect inwardly to secure the respective tubing to the respective nozzle adapter,

wherein the at least one trough of each of the inflow housing and the outflow housing is configured to accommodate spreading of the respective tubing when the respective tubing is coupled to the respective housing.

2. The assembly according to claim 1, wherein each housing base includes a plurality of concentrically-spaced troughs defined therein.

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- 3. The assembly according to claim 1, wherein each funnel-shaped inner surface includes a proximal portion, a distal 5 portion, and a transitional portion having sloping walls at a first predetermined angle.
- **4.** The assembly according to claim **3**, wherein each prone of each plurality of prongs includes a tapered portion at a distal end thereof, the tapered portion having a tooth-shaped 10 feature configured to engage the respective tubing.
- 5. The assembly according to claim 4, wherein the tapered portion is tapered at a second predetermined angle that is larger than the first predetermined angle thereby providing for deflection of each prong of the plurality of prongs upon insertion into the respective housing.
 - 6. The assembly according to claim 1, further comprising: a plurality of box clips coupled to respective ones of each of the plurality of prongs, wherein each box clip of the plurality of box clips is configured to deflect upon insertion into the respective housing and to interface with a corresponding window defined within the respective housing.
- 7. The assembly according to claim 1, wherein the inflow housing and the outflow housing share a common housing 25 portion disposed between the axes thereof.
- 8. The assembly according to claim 7, wherein the inflow wedge coupling and the outflow wedge are each configured to contact the common housing portion upon insertion of the respective wedge coupling into the respective housing.

* * * * *

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